Dynamics of a recurrent network of spiking neurons before and following learning

Daniel J. Amit\(^a,b\); Nicolas Brunel\(^c\)

\(^a\) Istituto di Fisica, Universita di Roma La Sapienza, Rome, Italy
\(^b\) Racah Institute of Physics, Hebrew University, Jerusalem, Israel
\(^c\) LPS, Ecole Normale Superieure, Paris Cedex 05, France

Online Publication Date: 01 November 1997

To cite this Article: Amit, Daniel J. and Brunel, Nicolas (1997) ‘Dynamics of a recurrent network of spiking neurons before and following learning’, Network: Computation in Neural Systems, 8:4, 373 — 404

To link to this article: DOI: 10.1088/0954-898X/8/4/003
URL: http://dx.doi.org/10.1088/0954-898X/8/4/003

Full terms and conditions of use: http://www.informaworld.com/terms-and-conditions-of-access.pdf

This article maybe used for research, teaching and private study purposes. Any substantial or systematic reproduction, re-distribution, re-selling, loan or sub-licensing, systematic supply or distribution in any form to anyone is expressly forbidden.

The publisher does not give any warranty express or implied or make any representation that the contents will be complete or accurate or up to date. The accuracy of any instructions, formulae and drug doses should be independently verified with primary sources. The publisher shall not be liable for any loss, actions, claims, proceedings, demand or costs or damages whatsoever or howsoever caused arising directly or indirectly in connection with or arising out of the use of this material.
Dynamics of a recurrent network of spiking neurons before and following learning

Daniel J Amit† and Nicolas Brunel‡
† Istituto di Fisica, Universita di Roma La Sapienza, Rome, Italy, and Racah Institute of Physics, Hebrew University, Jerusalem, Israel
‡ LPS, Ecole Normale Superieure, 24, rue Lhomond, 75231 Paris Cedex 05, France§

Received 9 April 1997

Abstract. Extensive simulations of large recurrent networks of integrate-and-fire excitatory and inhibitory neurons in realistic cortical conditions (before and after Hebbian unsupervised learning of uncorrelated stimuli) exhibit a rich phenomenology of stochastic neural spike dynamics and, in particular, coexistence between two types of stable states: spontaneous activity upon stimulation by an unlearned stimulus, and ‘working memory’ states strongly correlated with learned stimuli. Firing rates have very wide distributions, due to the variability in the connectivity from neuron to neuron. ISI histograms are exponential, except for small intervals. Thus the spike emission processes are well approximated by a Poisson process. The variability of the spike emission process is effectively controlled by the magnitude of the post-spike reset potential relative to the mean depolarization of the cell. Cross-correlations (CC) exhibit a central peak near zero delay, flanked by damped oscillations. The magnitude of the central peak in the CCs depends both on the probability that a spike emitted by a neuron affects another randomly chosen neuron and on firing rates. It increases when average rates decrease. Individual CCs depend very weakly on the synaptic interactions between the pairs of neurons. The dependence of individual CCs on the rates of the pair of neurons is in agreement with experimental data. The distribution of firing rates among neurons is in very good agreement with a simple theory, indicating that correlations between spike emission processes in the network are effectively small.

1. Introduction

Modelling the dynamical activity in cortex is becoming increasingly realistic, so much so as to allow direct comparison with data from single- and multiple-electrode recordings. The comparison includes, beyond mean spike rates in spontaneous and in selective activity, also single-cell spike statistics and cross correlations (Amit et al. 1994, Softky and Koch 1993, Usher et al. 1994, Tsodyks and Sejnowski 1995, Hansel and Sompolinsky 1996, Ben Yishai et al. 1995). The question that naturally poses itself is: how much complexity of the neural elements and how much specific structure of the neural assembly are actually indispensable for the reproduction of the experimental data? Most of the work cited above has dealt with visual cortex, where data are more accessible and hypotheses about geometric connectivity structure are plausible. Moreover, in visual cortex neural dynamics is investigated in the presence of visual stimuli, which in turn relate to the assembly structure via receptive fields and tuning properties of cells.

The present study has been motivated by delay activity in associative cortex (Miyashita 1993, Wilson et al. 1993, Goldman-Rakic et al. 1990, Fuster 1995). Such delay activity could

§ Laboratory associated with CNRS and Universities of Paris 6–7.
be sustained by the synaptic efficacies formed during training and hence its study relates directly to learning (Amit et al. 1994, Amit 1995). In IT cortex, following an unlearned stimulus, the spike rates are all low, while a familiar stimulus (i.e. one used during training) generates enhanced delay activity in some 1% of the cells (Miyashita 1988). Both types of 'states' are maintained, in the absence of the provoking stimulus, by the same set of synaptic efficacies in the same cortical module (column). In this area receptive fields are very large (Gross et al. 1972). Yet, for delay activity, one does observe columnar compartmentalization (Miyashita 1993). The lack of obvious geometric organization allows one to raise questions about the generic features of the assembly dynamics. Apart from the intrinsic interest in the computational properties of associative cortex, it is of basic importance to know which features of neural dynamics, in vivo, actually depend on a higher level of modelling complexity.

A theory of neural activity in a cortical module (Amit and Brunel 1997, to be referred to as AB97) has been shown to capture the expected spontaneous activity and 'working memory' states at the level of mean spike rates, as well as the coexistence of the two. The theory predicts average firing rates in different neuronal populations, and in different network 'states', as a function of the parameters describing the model neurons and the 'anatomy' of the network. However, there are other measured 'observables' which are not captured by it: firing rate distributions; interspike interval distributions; cross-correlations between spike emission times of different neurons. In this article, we investigate the behaviour of these 'observables' in a network of excitatory and inhibitory integrate-and-fire neurons, and whether a 'microscopic' dynamic network of interacting spiking neurons, in the presence of correlations, is well approximated by the theory of AB97.

1.1. Preparation: overview of the cortical module

1.1.1. 'Anatomy' of the module. Theory (AB97) has shown that the crucial parameters governing the stability of spontaneous activity are the level of non-selective stochastic excitatory afferent on the neurons of the module from outside the module and the relative strengths of geometrically unstructured excitation and inhibition within the module. Both parameters are related to the columnar organization observed in experiment and underlying the model. Functional columns of the dimension of 1 mm² parallel to the cortical surface appear in different parts of cortex. This corresponds to the anatomical findings that collateral connections between pyramidal cells as well as the ramification of the processes of inhibitory interneurons have this length scale in common (Braitenberg and Schütz 1991). In such a column there are about 10⁵ pyramidal cells and some 2 × 10⁴ interneurons.

Even when a column appears to be acting relatively autonomously, it remains an open system in two senses. First, it receives selective external afferents, either during the presentation of stimuli or from selective activity in other modules. Second, since at least one half of the afferent excitatory synapses of a typical pyramidal cell come from outside the local neighborhood (Braitenberg and Schütz 1991, Liley and Wright 1995), spontaneous activity in remote parts of the cortex alone, is a source of a high influx of spikes into a module (Bernander et al. 1991, Rapp et al. 1992, Amit and Tsodyks 1992, Shadlen and Newsome 1994, AB97). This second component we model by a random non-selective afferent to each synapse, representing the activity of neurons outside the module: a Poisson process with a rate equal to the mean spontaneous activity of excitatory neurons inside the module.

It represents a source of stochasticity in the dynamics of the module itself. The reason we model this afferent to be stochastic is an expression of our ignorance, not only of what
the rest of the brain does, but also of the interactions of the brain with the outside world. Clearly, had all these been known, the system might have been considered deterministic, or almost so. At a still lower level there would be the stochastic effects due to temperature, which are an expression of yet another level of openness and unknown interactions with the outside world. This non-selective flux is purely excitatory, because inhibitory neurons have local axonal ramifications, hence it has a fluctuating depolarizing effect on all cells in the module.

The other important parameter is local: the relative magnitude of overall local excitatory and inhibitory inputs to a cell. Stability requires (AB97) that local inhibition at least balance local excitation. A similar constraint appears in other studies (Shadlen and Newsome 1994, Tsodyks and Sejnowski 1995). Balancing excitatory and inhibitory inputs on the local level, in the face of an inhibitory population deficit of a factor of 4 or 5, implies that the average inhibitory afferent must be significantly stronger than the excitatory one, as already noted by Shadlen and Newsome (1994). This can be achieved in a variety of ways, which all have some empirical support: by more efficient synapses; by more reliable synapses or by higher inhibitory spike rates (Mountcastle et al. 1969, McCormick et al. 1985, Komatsu et al. 1988, Lacaille 1991, Thomson et al. 1993a, b).

1.1.2. Network sizes and scaling. The simulations reported here were run on an IBM RISC workstation. This limits the size of the networks to 15,000 cells. Since afferent spike statistics and fluctuations are essential for reproducing activity distributions as seen in cortex, various quantities must be scaled to make up for the fact that the simulated networks are smaller than the estimated 100,000 cells in a cortical column. This we do in two ways:

- By increasing the probability of connection between neurons in the module.
- By increasing neural spike rates.

For example, in a network of 100,000 neurons, with connectivity level of 5% and average rate of 5 spikes s\(^{-1}\) (hereafter abbreviated to s\(^{-1}\)), a neuron receives, on average, 250 spikes in 10 ms from recurrent collaterals. Simulating a network of 10,000 neurons, one could use a connectivity level of 20% and an average rate of 12.5 s\(^{-1}\) to obtain the same afferent spike number statistics. To check the effect on the network’s dynamics of decreasing the connectivity level and the average firing rates, we have performed a small number of simulations with larger networks, some as large as 10\(^5\) neurons.

1.1.3. Integrate-and-fire (IF) neurons. A simple model of a spiking neuron is the integrate-and-fire (IF) neuron (Knight 1972). It allows large scale simulations (thousands and even tens of thousands of neurons) and permits analytical estimates (see, e.g., Tuckwell 1988, Amit and Tsodyks 1991, 1992, AB97). Such a neuron, though very simple, when receiving noisy inputs has temporal dynamics similar to those of a complex reconstructed pyramidal neuron (Softky and Koch 1993). Amit and Tsodyks (1992) have shown how to reduce a neuron with arbitrary geometry, governed by non-linear cable equations, to an IF neuron with renormalized parameters. Thus it may not be necessary to model the individual neuron in great detail for the restricted set of observables at hand. In many cases the simplified models and more detailed ones reach similar conclusions regarding network dynamics (see, e.g., models of orientation selectivity in visual cortex: Tsodyks and Sejnowski 1995, Somers et al. 1995). To what extent identifiable dynamical behaviour of single neurons in a cortical environment depends on detailed ion-channel dynamics is one of the subjects we shall try to address in this study, through a comparison of our results with more complex models.
1.1.4. Synaptic structure—sources of disorder. Neurons are connected by synapses, of which the local collateral ones are explicitly modelled. Whether the network is in its ‘vacuous’ state, in which it can sustain only non-selective spontaneous activity, or in its instructed state, in which synapses have been modified by learning from stimuli, and structured delay activity can be sustained, there are several sources of disorder in the synaptic structure. They play an essential role in what follows. The main division line of the synaptic sources of disorder is between disorder which is fixed on time scales long compared with the internal neural time constants and fast-changing for which synaptic efficacies can fluctuate on very short time scales. The model contains three types of disorder, which can each be fixed or variable:

1. ‘Transmission probability’. This is the probability \( \epsilon \) that a spike emitted by a neuron reaches another randomly chosen neuron. Its fixed version is the ‘connectivity level’ \( c \), i.e. the probability of forming a (fixed) synapse between any pair of neurons in the column. The variable version is ‘reliability’, i.e. the probability \( r \) that a presynaptic spike arriving at a given existing synapse generates a postsynaptic potential (PSP) (see, e.g., Thomson et al 1993a, b, Tsodyks and Sejnowski 1995). The transmission probability is a product of these two parameters, \( \epsilon = cr \).

2. Random efficacy distribution. The efficacies vary from synapse to synapse.

3. Synaptic transmission delays. Each existing synapse has an associated delay between a presynaptic spike and the PSP produced by it. These delays vary from synapse to synapse with a given average and variability. Both synaptic efficacies and delays are either fixed (expressing the intrinsic variability of synapses due for example to their different positions on the dendrite) or fluctuating during the operation of the network (expressing fast synaptic noise).

1.2. Summary of results

The network was studied in two modes of operation:

1. Prior to learning. Synapses are totally random and we expect spontaneous non-selective activity.

2. Following Hebbian learning of external stimuli. Excitatory synapses potentiated by stimuli on top of the previous random distribution. We expect unstructured spontaneous activity following stimulation by an unfamiliar stimulus; and stimulus-selective delay activity following stimulation correlated with one of the previously learned stimuli (AB97).

1.2.1. Unstructured network.

1. Simulations versus theory (figure 2). The distributions of firing rates measured in the simulations are in very good quantitative agreement with the theory (AB97), as well as the regions of parameters in which the various activity states are stable. The rate distributions are typically wide, due to the variability in the number of connections from neuron to neuron. The fact that a simple theory accurately reproduces the results of simulations has the important consequence that given the constitutive parameters of the network, the ‘state’ it reaches, in terms of spike-rate distributions in its different populations, can easily be predicted for large networks for which numerical simulation is not practicable.
2. **Firing is nearly Poisson (figure 6).** The distribution of interspike intervals (ISI) in the emission process of single cells is similar to a Poisson process, except at small intervals. The variability in the spike emission process is high for low rates and is effectively controlled by the value of the post-spike reset potential relative to the average depolarization of the membrane.

3. **Large global activity fluctuations and CCs (figures 3, 4, 5 and 11).** The global activity in the network has very large, short lived, fluctuations. The total number of emitted spikes increases several times above average and is then suppressed by rising inhibition. This results in a pronounced peak at zero delay in the CCs of the spike trains of any pair of neurons in the network. The size of the peak in the average CCs relative to the background increases when average firing rates decrease, at fixed transmission probability, and decreases linearly with the transmission probability, at fixed average rates. These CCs typically exhibit damped oscillations, with a frequency controlled by synaptic delays and conductance change time constants.

4. **CCs have small influence on rates.** In the range of parameters studied, the size of the peak in the CC has small influence on mean spike rates. Hence, the existing correlations between spike processes on different cells are effectively small. We also expect this to be the case in a cortex.

5. **CCs of individual pairs of neurons depend very weakly on synaptic efficacies connecting the pair (figure 7).** They are essentially indistinguishable for two neurons that are mutually connected, have a one way connection or no connection. Individual CCs depend more strongly on firing rates of the two cells: neurons with lower rates are typically more correlated than neurons with high rates.

1.2.2. **Networks structured by learning—selective activity (figures 9 and 10).** Detailed description of network dynamics following Hebbian learning will be presented in a future communication. Here we limit ourselves to an example. Learning consists of stochastic LTP in synapses among pairs of excitatory neurons simultaneously driven by a stimulus and LTD among neurons, of which one is driven and one is not.

1. If potentiation is not strong enough, no selective delay activity appears, but spontaneous activity becomes inhomogeneous: all neurons which responded to any one of the stimuli increase their rates, while other neurons decrease their spontaneous rates.

2. Beyond a critical potentiation level, the spontaneous activity state coexists with a multiplicity of selective ‘working memory’, or delay activity, states. The spontaneous activity distribution is excited by any stimulus different enough from all the stimuli previously learned (see, e.g., figure 1 of Miyashita 1988). Following a stimulus similar to one of the learned stimuli, the network maintains a stationary distribution of spike rates in which a small selective group of cells has significantly elevated rates which persist following the removal of the stimulus (delay activity). Most of the neurons in the module emit spikes at low rates.

3. The average firing rates of neurons which participate in a given excited state can be relatively close to the spontaneous rates (typically there is a ratio of 4:1 to 10:1). These ratios are similar to, though slightly higher than, those observed in the delay experiments in primate cortex (see, e.g., Wilson et al 1993, Nakamura and Kubota 1995).

These phenomena are well captured by theory (AB97).
2. Methods

2.1. Details of the model

2.1.1. Network architecture. We study a network composed of \( N \) neurons, from which \( N_E = 0.8N \) are excitatory and \( N_I = 0.2N \) inhibitory. Each neuron in the network has a probability \( c \) (connectivity level) of a direct synaptic contact with any other neuron (excitatory or inhibitory). Hence each neuron receives on average \( cN_E \) recurrent excitatory synapses, and \( cN_I \) recurrent inhibitory synapses. This leads to an amorphous recurrent synaptic structure. Each neuron receives an unselective stochastic afferent representing the synaptic input from spontaneous activity in remote parts of cortex. In the simulations \( N \) varied between 6000 and 15 000 for networks with fixed synapses and up to 100 000 for networks with fluctuating synapses (see below) and ‘transmission probabilities’ \( \epsilon \) between 0.05 and 0.25.

2.1.2. Neurons. Excitatory and inhibitory neurons are modelled as IF cells. Neuron number \( i \) of type \( \alpha \) (\( i = 1, \ldots, N_\alpha; \alpha = E, I \)) has, at time \( t \), two dynamical variables associated with it: a depolarization at the soma \( V_\alpha^i(t) \) and an afferent postsynaptic current at the somatic integrator \( I_\alpha^i(t) \). It is parametrized by an integration time constant \( \tau_\alpha \); a threshold \( \theta \); a post-spike reset potential \( V_r \) and an absolute refractory period \( \tau_0 \). (The last three are taken as being equal for all neurons.)

The membrane depolarization of a neuron of type \( \alpha \), below threshold, is modelled by

\[
\tau_\alpha \dot{V}_i = -V_i + I_i
\]

with the synaptic current \( I_i \) expressed in units of the potential. When \( V_i \) reaches the threshold \( \theta \), the neuron emits a spike and its potential is reset to \( V_r \), following an absolute refractory period \( \tau_0 \). \( I_i \) is the sum of the recurrent synaptic input \( I_{\text{rec}}^i \) and the external synaptic input \( I_{\text{ext}}^i \). Assuming that the synaptic conductance dynamics is fast relative to the neural integration time, the net recurrent depolarizing synaptic input charging the membrane of neuron \( i \) at time \( t \) (see, e.g., AB97) is

\[
I_{\text{rec}}^i(t) = \sum_{j \in E,k} \rho_j(t) J_{ij} \tau_\alpha \delta(t - \tau_{ij} - t_k^j) - \sum_{j \in I,k} \rho_j(t) J_{ij} \tau_\alpha \delta(t - \tau_{ij} - t_k^j)
\]

where the reliability variable \( \rho_j(t) = 1 \) with probability \( r \) and is 0 otherwise, independently at every synapse and for every spike (see also Tsodyks and Sejnowski 1995). \( J_{ij} \) is the synaptic efficacy from neuron \( j \) to neuron \( i \), \( \tau_{ij} \) is the delay associated with this synapse, and \( t_k^j \) is the time neuron \( j \) emitted spike number \( k \). The summations are over \( j \in E (I) \), i.e. over excitatory (inhibitory) presynaptic neurons and over the spikes \( k \), arriving at a particular synapse. \( J_{ij} \) is the amplitude of the PSP provoked in neuron \( i \) by a spike arriving at this synapse. The synaptic variables will be defined in more detail below.

We take \( \tau_E = 10 \) ms, \( \tau_I = 5 \) ms, to express the fact that inhibitory neurons are typically faster than excitatory ones. \( \theta = 20 \) mV above resting potential, \( V_r = 10 \) mV (except in subsection 3.2), \( \tau_0 = 2 \) ms.

2.1.3. Recurrent synaptic interactions. Synapses in the network are of four possible types, as each of the presynaptic and postsynaptic neurons can be either excitatory or inhibitory. A synaptic quantity labelled \( \alpha\beta \), connects a presynaptic neuron of type \( \beta \) to a postsynaptic neuron of type \( \alpha \). Synapses are drawn at random according to one of the following procedures:
A. **Fixed random connectivity.** Every neuron receives an equal number of contacts, from $cN_E$ excitatory and $cN_I$ presynaptic neurons, chosen at random.

B. **Variable random connectivity.** A synapse between any pair of neurons is present with probability $c$ independently for all pairs of neurons. The number of contacts a neuron receives is a binomial random variable with mean $cN_E$ ($cN_I$) and RMS $\sqrt{c(1-c)N_E}$ ($\sqrt{c(1-c)N_I}$), for excitatory (inhibitory) contacts, respectively.

In the simulations both procedures have been tested. Procedure A is best suited for comparison with the previous analysis (AB97), since it makes all neurons equivalent with respect to the connectivity scheme. The analysis can be extended to include variability in the connectivity (see appendix B). The efficacy of the synapse transmitting from neuron $j$ to $i$ is denoted $J_{ij}$. If $(ij)$ are of types $\alpha\beta$, its value is chosen from a Gaussian distribution $\rho_J$ with mean $J_{\alpha\beta}$ and width $J_{\alpha\beta}\Delta$. The delay associated with synapse $(ij)$, $\tau_{ij}$, is chosen at random from a uniform distribution $\rho_d$ with mean $\tau_d$ ranging between $(1 - s_d)\tau_d$ and $(1 + s_d)\tau_d$.

Finally, there may be fast (annealed) synaptic disorder, i.e. (i) each synapse has reliability $r$: when presynaptic neuron $j$ emits a spike, it provokes a PSP in the postsynaptic neuron $i$, of magnitude $J_{ij}(0)$, with probability $r (1 - r)$, respectively; (ii) when a spike arrives at a postsynaptic neuron, its efficacy and delay are drawn randomly from distributions $\rho_J$ and $\rho_d$ respectively, independently for different spikes. This type of disorder allows for the simulation of larger networks.

We have simulated networks in the following parameter ranges:

- **Synaptic efficacies:**
  - excitatory to excitatory, $J_{EE}$, 0.1 to 0.5 mV;
  - inhibitory to excitatory, $J_{EI} = 3J_{EE}$ (0.3 to 1.5 mV);
  - excitatory to inhibitory, $J_{IE} = 2J_{EE}$ (0.2 to 1 mV);
  - inhibitory to inhibitory, $J_{II} = 3J_{IE}$.

The excitatory to excitatory efficacies are in the range of experimentally observed average values (e.g. Mason *et al* 1991). The ratio of inhibitory to excitatory average efficacies was set to three in order to have a stable spontaneous activity state with low rates. This results in larger IPSP values. Given the desired values of stable rates in different populations of neurons and the ratios of inhibitory to excitatory efficacies, the precise values of the synaptic efficacies used in the simulations are calculated by the theory (AB97).

- **Variability of synaptic efficacies, $\Delta$, in the range 0 to 0.5.**
- **Spike transmission delay, $\tau_d$, average 1 ms, $s_d = 0.5$.**
- **Synaptic reliability, $r$, in the range 0.05 to 1.**

There are two limiting cases:

- **Fixed random (‘quenched’) synaptic structure.** The connectivity level $c$ varies from network to network. For each network the synaptic system and the delays are fixed, i.e. the reliability parameter $r = 1$.

- **Variable random (‘annealed’) synaptic structure.** The reliability parameter $r$ varies from network to network. The connectivity level $c = 1$ (all-to-all connections). Both synaptic efficacies and delays are selected at random and independently at each step. The entire synaptic structure fluctuates in time and is uncorrelated at different time steps.

### 2.1.4. Non-selective external input.

Each neuron in the local module receives a non-selective, stochastic external input. It represents the background activity of other cortical
areas that provide inputs to the network. The rates of the excitatory neurons in these areas are assumed to be similar, on average, to the rates of the neurons in the local network. Moreover, the efficacies of the synaptic connections from outside the network are assumed to be, on average, equal to the recurrent excitatory connections on the same neurons.

If no stimulus is presented to the network, the total external current to neuron \( i \) between \( t \) and \( t + dt \), \( I^\text{ext}_i = I^* \), is chosen randomly and independently at each neuron and each time step, according to

\[
I^*_i(t) = J_{aE} \mathcal{N}_i(t)
\]

where \( \mathcal{N}_i \) is drawn from a Poisson distribution with mean \( \epsilon N_E \nu_E dt \), and \( \nu_E \) is the average spontaneous spike rate of excitatory neurons within the module. In other words, the non-selective external input to a cell is equal, on average, to the input it would receive, in the same time interval, from local collaterals that are firing at spontaneous rates.

### 2.1.5. Structured external input–external stimuli

For simplicity each of the \( p \) stimuli is characterized by an \( N_E \)-bit word, \( \eta^\mu_i = 0, 1 \) (\( i = 1, \ldots, N_E, \mu = 1, \ldots, p \)), in which the 1-bits define a subset of the excitatory neurons which are activated by stimulus \( \mu \). Each stimulus activates a random, and uncorrelated, subset of \( f N_E \) excitatory neurons. \( f \) is the coding level, or sparseness, of a stimulus in the module. When stimulus number \( \mu \) is presented, the external currents \( I^\text{ext}_i \) become

\[
I^\text{ext}_i(t) = I^*_i(t) (1 + H \eta^\mu_i)
\]

where \( H \) is the selective ‘contrast’ of the stimulus with respect to the background. The response of a cell during the presentation of a stimulus is its ‘visual response’.

\( H \) is typically small, between 0.1 and 0.2. It is spontaneous activity, which maintains neurons most of the time depolarized near threshold, that produces a sensitivity to stimuli with low contrast (see also Tsodyks and Sejnowski 1995).

### 2.1.6. Learning

The presentation of stimuli induces modifications in the synapses of the unstructured network, whose behaviour is simulated and described first. Upon learning, starting from its initial state \( J_{ij} \), a synaptic efficacy may either remain unmodified, or make transitions to one of two possible states: a potentiated state \( J_{ij} + \delta J_+ \), and a depressed state \( J_{ij} - \delta J_- \). Thus any synapse has three possible states; the state eventually chosen depends on the history of stimuli presentations. Possible transitions between these states are:

- Potentiation (LTP), the transition from either \( J_{ij} \) or \( J_{ij} - \delta J_- \rightarrow J_{ij} + \delta J_+ \), occurs with probability \( q_+ \) if both pre- and postsynaptic neurons are activated by a given stimulus (i.e. \( \eta_i = \eta_j = 1 \) for the particular stimulus);
- Depression (LTD), the transition from either \( J_{ij} \) or \( J_{ij} + \delta J_+ \rightarrow J_{ij} - \delta J_- \), occurs with probability \( q_- \) if either the presynaptic or postsynaptic neuron is activated by the stimulus (but not both).

Otherwise no transition occurs (see, e.g., Amit and Fusi 1994, Amit and Brunel 1995). Note that once a synapse has made a transition it cannot go back to its initial state \( J_{ij} \). Such simplified dynamics schematizes roughly experimental observations about synaptic plasticity in neocortex (see, e.g., Bliss and Collingridge 1993, Artola and Singer 1993). The synaptic dynamics is not explicitly modelled. Instead, we consider a situation in which the \( p \) stimuli have already been presented a large number of times (overtraining) in a random sequence. In this case, the probability distribution of the resulting synaptic efficacies as a function of the \( p \) stimuli can be computed explicitly (Brunel et al. 1997). The result is given
in appendix C. In the resulting synaptic matrix, the potentiated efficacies have an average value of \( J_1 = J_{EE} + \delta J_+ \), and the depressed ones an average value of \( J_0 = J_{EE} - \delta J_- \), where \( J_{EE} \) describes the unstructured network. In the example shown in section 3, the number of stimuli was \( p = 24 \), the coding level (sparseness) \( f = 0.083 \), \( J_1 = 2.2 J_{EE} \), \( J_0 = 0.8 J_{EE} \).

2.2. Theoretical estimates of stable rate distributions.

Here we briefly recapitulate the results of the analysis for comparison with simulations. For technical details see AB97 and appendix A. The assumptions are:

1. Each neuron receives a large number of spikes in an interval corresponding to its integration time period.
2. The depolarization caused by a single spike is small compared to the threshold.
3. Spike emission times of different neurons are uncorrelated, although their rates may be correlated.

Under these assumptions one can approximate the synaptic input of a neuron by a Gaussian diffusion process, whose mean and variance density can be derived as a function of the average spike rates of excitatory and inhibitory neurons, the average synaptic efficacies and their variability, the number of afferent excitatory and inhibitory connections, and the integration time constant of the neuron.

From these data one deduces the average firing rate of both types of neurons in the local module, as a function of the mean and variance of the input received by the neuron. Since these moments depend in turn on the average rates, the analysis deduces self-consistent equations giving spontaneous self-reproducing average firing rates in the network (see appendix A). The stability analysis shows that for realistic rates of spontaneous activity, of the order of \( 1-5 \) s\(^{-1} \), to be stable, inhibition has to be stronger than some critical value depending on the ratio of the integration time constants of excitatory and inhibitory neurons. The theory was then extended to the case in which learning occurs in the column. It is found that ‘working memory’ states, representing the stimuli presented during training to the network, can be stable in the absence of the stimulus, provided Hebbian potentiation is strong enough. This simple theory was used to select parameter regions for the simulations. In all cases where analysis predicted stable dynamics the full simulations were stable and produced the expected average rates.

The analysis (AB97) was carried out, for simplicity, in a situation in which all neurons receive the same number of connections. It has been extended to the case in which the number of connections varies from neuron to neuron, leading to a wide distribution of firing rates in the network. The equations for both average firing rates and their distribution are presented briefly in appendix B. They will be described in more detail elsewhere.

2.3. Simulation procedure, recordings and display.

In the simulation the neural dynamics, equation (1), is discretized and the membrane potential at \( t + \Delta t \) is given by

\[
V_i(t + \Delta t) = \left( 1 - \frac{\Delta t}{\tau_a} \right) V_i(t) + \frac{\Delta t}{\tau_a} \left( I_{rec}^i(t) + I_{ext}^i(t) \right) \tag{4}
\]

\[
I_{rec}^i(t) = \frac{\tau_a}{\Delta t} \left\{ \sum_{j \in E} \rho_j(t) J_{ij} S_j(t - \tau_{ij}) - \sum_{j \in I} \rho_j(t) J_{ij} S_j(t - \tau_{ij}) \right\} \tag{5}
\]
which yields

$$V_i(t + dt) = \left(1 - \frac{dr}{\tau_a}\right)V_i(t) + \sum_{j \in E} p_j(t) J_{ij} S_j(t - \tau_{ij}) - \sum_{j \in I} \rho_j(t) J_{ij} S_j(t - \tau_{ij}) + \frac{dr}{\tau_a} I_{i,\text{ext}}. \quad (6)$$

in which the delays, $\tau_{ij}$, are in units of $dt$, and the external input, $I_{i,\text{ext}}$, is given by equation (3). If in $t + dt$ $V_i$ reaches threshold, the neuron emits a spike, as indicated by a spike activation variable $S_i(t) (= 0, 1)$. The integration step $dt$ was $0.01-0.05\text{ ms}$ for both types of neurons, an interval in which on average a neuron receives less than one spike. Lowering $dt$ further does not significantly modify the results.

The duration of the runs varied between $200\text{ ms}$ (short test runs) and $3\text{ minutes}$ in real neural time, as fixed by setting the absolute refractory period to $2\text{ ms}$.

The simulations of the unstructured network were carried out as follows:

1. The synaptic structure was set up according to the procedure defined in ‘Recurrent synaptic interactions’ above.

2. The initial depolarization of the neurons was drawn from a Gaussian distribution of mean and variance given by assuming that spike emission processes of different neurons are independent Poisson processes with the expected spike rates (AB97 and appendix A) truncated at the neural threshold $\theta$. We checked that choosing different distributions (for example, all neurons initially at resting potential) leads to the same results, apart from a transient period of about $50\text{ ms}$.

3. At each time step of the simulation the states of all neurons are updated according to equation (6), and the following observables are recorded:
   - **Global activity.** The total number of spikes in excitatory and inhibitory populations in $dt$ at time $t$:
     $$n_{E,I}(t) = \sum_{i \in E,I} S_i(t). \quad (7)$$
   - **Single-neuron recordings.** Spike times and depolarization of a subset of randomly chosen neurons (20 excitatory and 10 inhibitory).

At the end of a run we calculate the population averages of the rates, $\nu_{E,I}$, for excitatory and inhibitory networks:

$$\nu_{E,I} = \frac{1}{N_{E,I} T dt} \sum_{t = 1}^{T} n_{E,I}(t). \quad (8)$$

From the global activity at each time step we compute the average cross-correlation (CC) between a pair of neurons, one of type $\alpha$ and one of type $\beta$:

$$C_{\alpha\beta}(\tau) = \frac{1}{N_\alpha N_\beta (T - \tau)} \sum_{t = 1}^{T - \tau} n_\alpha(t)n_\beta(t + \tau) \quad (9)$$

where $T$ is the length of the run in units of $dt$.

Asymptotically, for large $\tau$, the average CC, equation (9), tends to $(\nu_\alpha dt)(\nu_\beta dt)$, with $\nu_\alpha$ the mean rate in population $\alpha$. This background value is used in what follows as a normalization, dividing the right-hand side of equation (9).

Single-cell recordings are visualized as in physiological experiments—spike times as rasters and depolarizations as continuous curves. From the spike times of cell $i$ we compute its spike rate, $\nu_i$, averaged over an interval $T$ as

$$\nu_i = \frac{1}{T dt} \sum_{t = 1}^{T} S_i(t)$$
which gives the population distribution of rates, and its ISI (inter spike interval) histogram.

From the spike times of a given pair of cells $i$ and $j$ we compute the cross-correlation (CC) of their spike trains, defined as

$$C_{ij}(\tau) = \frac{1}{T-\tau} \sum_{t=1}^{T-\tau} S_i(t) S_j(t+\tau).$$  \hspace{1cm} (10)

Averaging $C_{ij}$ over all pairs of cells, one of type $\alpha$ and one of type $\beta$, one recovers the average cross-correlation $C_{\alpha \beta}$, equation (9), i.e.

$$C_{\alpha \beta}(\tau) = \frac{1}{N_\alpha N_\beta} \sum_{i \in \alpha, j \in \beta} C_{ij}(\tau)$$

which was expressed above in terms of the global activities. $C_{\alpha \alpha}$ is the autocorrelation of the global activity in population $\alpha$.

3. Results

3.1. Spontaneous activity—a typical example

We start with a network of $N = 7500$ neurons, of which $N_E = 6000$ and $N_I = 1500$. The parameters of the network are summarized in table 1. The connectivity, $c = 0.2$, is fixed random. The synaptic parameters were determined by theory (AB97) to obtain expected average spontaneous rates of $\nu_E = 13 \text{s}^{-1}$ and $\nu_I = 25 \text{s}^{-1}$. The rates are high to compensate for the small size of the network. The statistics of the excitatory afferent input here would be the same as in a network with an average of 8000 recurrent excitatory connections per neuron and an average excitatory rate of 2 \text{s}^{-1}. In a stationary situation, each excitatory neuron receives about 160 recurrent excitatory spikes, 160 excitatory external spikes, and about 80 inhibitory spikes per $\tau_\ell (= 10 \text{ ms})$. Each inhibitory neuron receives about half these numbers per $\tau_I$, because of its shorter time constant.

Figure 1 presents the ‘intracellular’ recordings of the depolarization of randomly chosen neurons (four excitatory and one inhibitory), and the spike rasters of randomly selected (20

<table>
<thead>
<tr>
<th>Table 1. Parameters used in the simulation of subsection 3.1.</th>
</tr>
</thead>
<tbody>
<tr>
<td><strong>Neuronal parameters</strong></td>
</tr>
<tr>
<td>$N$ (number of neurons)</td>
</tr>
<tr>
<td>$\tau$ (integration time constant, ms)</td>
</tr>
<tr>
<td>$\theta$ (threshold, mV)</td>
</tr>
<tr>
<td>$V_r$ (reset potential, mV)</td>
</tr>
<tr>
<td>Average frequencies predicted by theory (Hz)</td>
</tr>
<tr>
<td>Observed average frequencies (Hz)</td>
</tr>
<tr>
<td><strong>Synaptic parameters</strong></td>
</tr>
<tr>
<td>$J$ (average efficacy, mV)</td>
</tr>
<tr>
<td>$\Delta$ (relative width of distribution of efficacies)</td>
</tr>
<tr>
<td>$\epsilon$ (probability of connection)</td>
</tr>
<tr>
<td>$\tau_d$ (average delay, ms)</td>
</tr>
<tr>
<td>Average number of afferent spikes/$\tau$</td>
</tr>
</tbody>
</table>
Figure 1. (a)–(e) ‘Intracellular recordings’ of depolarization in a 500 ms sub-interval of the run. From top: four excitatory neurons and one inhibitory neuron. Dotted line, resting potential; dashed line, threshold. The size of the depolarization at the spikes is only a visual aid. (f) Spike rasters of 20 excitatory neurons. (g) Rasters of 10 inhibitory neurons.

excitatory and 10 inhibitory) simultaneously recorded neurons in 500 ms out of a 100 s run. The horizontal dotted line indicates the resting polarization and the dashed line is the threshold. The neurons are most of the time depolarized and emit spikes due to abrupt fluctuations.
3.1.1. Distribution of firing rates. Figure 2 is the most remarkable result of this study: the histograms of the measured spike rate distributions in the two populations of neurons (left, excitatory; right, inhibitory) are superposed on the theoretical predictions. This is not a fit of the results of the measurements (simulations), but the prediction of the theory, which given the parameters of table 1, gives the rate distribution via equations (B3)–(B5) of appendix B. A $\chi^2$ test shows that the measured rates are highly consistent with the theory. The rate of each neuron is the average over the entire (100 s) run. On average an excitatory neuron emits about 1300 spikes in this interval in an approximately Poisson process, the error in estimating the rate is about $\sqrt{1300}/100 \sim 0.36$ Hz, i.e. smaller than the bin size. A histogram using the first 50 s of the run is essentially indistinguishable from the one shown in figure 2.

The distributions have large widths, approximately equal to the average firing rate. It is mainly due to the variability in the number of connections received by the neurons. For large number of connections, the variability in the relative connectivity is low. Its effect on spike rates is 'magnified' by the fact that neurons are most of the time near threshold.

3.1.2. Global activity fluctuations and average cross-correlations. In an unstructured network the total number of excitatory and of inhibitory spikes emitted at any given time, determine the statistics of spike emission in the next moment. Hence, the dynamics of a network can be followed by viewing the time evolution of these two global variables, displayed in figure 3 (lower strips). One observes very large, sharp fluctuations which are underlined by comparison with the activity of a population of independent Poisson processes with the same average frequency as in the simulation (upper strip in each window, same scale). The statistical fluctuations, which appear also in the uncoupled Poisson population, are initially amplified by the cooperative dynamics of the network, and only later suppressed by the rising inhibition. If inhibition is significantly weaker, these fluctuations are further amplified and the activity distribution becomes unstable.
The ‘surges’ in the number of emitted excitatory spikes reach excitatory and inhibitory cells at about the same time and are amplified during the time in which inhibitory neurons integrate the afferent excitation, which is of order 5 ms. After this time, extra inhibition is activated and, if strong enough, suppresses the excitation. The inhibitory integration time is roughly the time scale of the sharp fluctuations. These fluctuations are reflected in the collateral contributions (excitatory and inhibitory) to the EPSPs received by neurons in the network. They are shown, for a randomly chosen excitatory neuron, in figure 4. The hyperpolarizing inhibitory contribution overpowers the recurrent excitation and both fluctuate with the global activity, figure 3.
Figure 5. Average CCs between E–E, E–I, and I–I neurons. Note the similarity between the three figures. In all three there is a central peak with the same amplitude relative to the background (between 1.5 and 1.6), and the same damped oscillations with a time constant of about 5 ms. The only difference is in the slight asymmetry of the E–I CCs, indicating that inhibitory neurons have a tendency to fire just after excitatory neurons. These CCs reflect the temporal structure of the global activity fluctuations, figure 3.

Note that the recurring surges of activity in this figure (on a time scale of 5–6 ms) do not imply a 200 Hz oscillation at the single-neuron level (though it might in local field potential). The surges are composed of sub-populations of neurons drawn essentially at random in each surge. This is corroborated by the absence of structure in the ISI histograms (figure 6).

The activity surges condition the structure of the cross-correlations of spike trains of pairs of neurons. If the number of spiking neurons surges much above average, the probability that any two neurons emit spikes within the short interval of the surge is higher than average. This, in turn, leads to a narrow peak near zero time difference in the CCs. These peaks are observed in all three average CCs in figure 5, together with a time scale of a damped oscillation of 5–6 ms, that can be interpreted as a degree of synchrony in the neuronal firing.

The structure of the CCs and the implied synchronization appear in contrast with the assumptions of independence underlying theory (AB97). Yet the fact that a simple theory assuming uncorrelated spike emission processes reproduces the rate distribution that well (figure 2) is a clear indication that these correlations are effectively small.

3.2. Single-cell spike statistics

Figure 6 shows the distribution of interspike intervals (ISI) of two randomly chosen neurons. The histograms are similar to the superposed ISI histogram of a Poisson process, apart from
the behaviour at small interspike intervals, which is due to refractory behaviour. The variability of ISI intervals, as measured by the ratio of the standard deviation to the mean of the distribution (CV in the figures), is somewhat lower than that of a Poisson process ($\approx 1$), though some neurons have $CV > 1$. Neurons with low firing rates have CVs larger than 1, while neurons with higher firing rates have CVs typically below unity.

The variability of spike emission can be accounted for by variations in the post-spike reset potential (Tsodyks et al 1994, Troyer and Miller 1997). We find that it is effectively controlled by the relative magnitude of the average depolarization of the neuron to the post-spike reset potential: if the average depolarization is below the post-spike reset potential, variability will be typically higher than 1, and vice versa. Variability decreases as rates increase, at constant $V_r$, because higher rates are accompanied by higher average depolarization.

We have simulated networks with two values of $V_r$ (10 mV and 15 mV). We measured the dependence of CV of one cell as a function of its average depolarization. The results are summarized in figure 6. At a given $V_r$, CV decreases when the average membrane potential increases. It is typically $> 1$ for cells depolarized, on average, below $V_r$, and $< 1$ for cells on average depolarized above $V_r$.

3.3. Cross-correlations

Cross-correlations are perhaps the most detailed quantity systematically measured in multiple unit recordings. We have studied the dependence of these quantities, in the collective state of spontaneous activity, as a function of various parameters.

3.3.1. Effect of individual neuronal parameters. In a network with parameters as in table 1, we investigated the dependence of the average CCs in each sub-population on the specifying parameters.
Effect of connectivity. The set of all recorded excitatory neuron pairs was divided into three subsets:

1. pairs reciprocally connected;
2. pairs with a one-way connection;
3. pairs without direct synaptic contact.

The average CC in each class was computed. The results are shown on the left of figure 7. It turns out that there is little difference between cross-correlations of these three types of pairs. Reciprocally connected neurons have slightly higher CCs than average. One-way connected neurons have slightly asymmetric CCs; however, the asymmetry is hardly noticeable, and would be extremely difficult to notice in an experimental situation (see below). Unconnected pairs have CCs indistinguishable from average CCs, just because the large majority of pairs are unconnected.

Effect of rates. All excitatory neuron pairs were divided into three subsets:

1. both cells with low rates ($< 10 \text{ s}^{-1}$);
2. both with high rates ($> 30 \text{ s}^{-1}$);
3. one with a low rate and one with a high rate.

Average CCs were computed in each sub-population, figure 7. One finds that neurons with low firing rates are typically more correlated than neurons with high firing rates. There is a slight asymmetry in the CCs of pairs with high–low rates, indicating that high rate neurons have a tendency to fire just before low rate neurons when surges of activity occur. Note that these effects are quite similar to those obtained in a network of Hodgkin–Huxley neurons.
Figure 8. Average cross-correlations between excitatory neurons, for $\tau_{\text{delay}} = 1$ ms (full curve), 2 ms (long-dashed) and 4 ms (short-dashed). Increasing the average delay increases the time constants of the damped oscillations, slowing down the observed oscillation frequency.

(Hansel and Sompolinsky 1996). All differences are much more pronounced than those due to connectivity.

3.3.2. Effect of time constants on the temporal structure of CCs.

Effect of synaptic transmission delays. We have performed simulations with average delays between 1–4 ms. Increasing average delays leads to a minor increase in the average rates, and a corresponding decrease of the relative central peak of the CC (see, e.g., discussion of effect of rates, above). By contrast, delays modify quite significantly the shape of the cross-correlations. Figure 8 shows the average cross-correlations in the excitatory population, for average delays $\tau_{\text{delay}} = 1, 2$ and 4 ms. Increasing delays decreases the damping factor of the oscillations, with a time constant that increases with the average delay. For example, with $\tau_{\text{delay}} = 4$ ms the time constant of the oscillation increases to about 40 ms. The reason is that for longer delays the network takes more time to ‘recover’ from big surges of activity.

Effect of synaptic conductance time constants. The time constants of synaptic conductance changes have an effect on the CCs similar to that of transmission delays. Simulations performed with finite conductance time constants produce similar ‘broadening’ of the CCs with increasing time constants, together with a reduction of the size of the central peak, at parity of rates. The introduction of a conductance time constant brings about a reduction of the peak of the CCs larger than that of delays, and it tends to damp the oscillations, rather than amplify them†.

† Note that the adjunction of finite time constants associated with synaptic conductance changes leaves intact the other results of the paper. The rate distributions can be described analytically replacing the function $\phi$ of equation (A7) by a transfer function taking into account these time constants (Brunel and Sergi 1997). The behaviour of the network associated with learning and memory also survives this step towards greater biological realism.
Effect of the ratio between inhibitory and excitatory time constants. The ratio between the integration time constants of inhibition and excitation also affects the temporal structure of CCs, since the reaction time of the inhibitory network to surges in the global activity varies. For example, a network similar to the one of table 1 but with $\tau_I = 10$ ms has a time scale of oscillations of about 20 ms. Decreasing the time constant of inhibition also provokes an increase in the size of the central peak of CCs at parity of rates.

In conclusion, varying different time constants in the network preserves the main qualitative features of the global activity fluctuations and correspondingly of the CCs. Quantitatively, the time constants of the damped oscillations can take a wide range of values (approximately from 5 to 40 ms, corresponding to frequencies of 25 to 200 Hz) depending on the value of the neuronal time constants. Further study is under way to complete the details.

3.3.3. Statistical significance of CCs. Cross-correlations shown in this paper were averaged over many pairs of neurons, so that the observed effects are highly significant. This is an advantage of the numerical simulations over neurophysiology, since a neurophysiologist must often evaluate the cross-correlation of single pairs of neurons, recorded over a limited time interval. For a discussion on statistical significance of CCs, see, e.g., Abeles (1991). To estimate with 99% confidence a peak in the CC (with a bin width $dt = 1$ ms) 33% above background, one would have to record a pair of neurons, with average rates of 10 Hz, for 10 minutes. Such a recording could detect the central peaks of CCs shown in figure 5, but not the secondary peaks. Thus, it is likely that the temporal structure would be undetected. A recording of 1 hour would enable one to detect peaks as small as 14% above background, but the secondary peaks of figure 5 would still be below the 99% confidence limit.

To infer the mere existence of a synaptic connection from the cross-correlations of single pairs of recorded neurons is even more difficult. First, since CCs depend strongly on rates one would first have to record simultaneously many neurons so as to have at least several pairs with the same rates. The recordings should be long enough as to detect a difference in the peaks of CCs of about 10% of the background. For the parameters used above this would imply a recording time of about two hours. Such estimates depend on the rates of both neurons and on the bin size used, but they are nevertheless useful to underline the potential difficulties in obtaining estimates from CCs in experimental conditions.

3.4. Learning and selective activity

We proceed with an example of the dynamics of the network following learning, to show its operation as an autoassociative memory, with two types of states, a ‘spontaneous activity’ state and ‘working memory’ states correlated with learned stimuli. Detailed description and analysis of the dynamics of instructed networks will be given elsewhere. It would make this account too long.

The parameters of the simulated network are given in table 2. Other parameters are as in table 1. The structured part of the synaptic matrix corresponds to over-training (repeated presentation) by $p = 24$ stimuli with coding level $\tilde{f} = 0.08$. This creates a synaptic distribution of the form described in subsection 2.1. The simulation represents the ‘testing’ phase, following the training. The protocol (bottom trace in figure 9) consists of: (i) 100 ms prestimulus interval, in which the network is in its spontaneous activity state; (ii) 100 ms presentation of one of the learned stimuli; (iii) stimulus removed, followed by a ‘delay’ interval of 300 ms out of 10 s in the actual simulation. We record and display both individual neurons and the evolution of global quantities.
The rasters of 30 neurons (20 excitatory and 10 inhibitory) in the first 500 ms of a simulation are shown in figure 9. Among the 20 excitatory neurons the top five are from the foreground of the presented stimulus (have ‘visual response’). The total activity, during the entire protocol, in four neural populations (excitatory foreground; excitatory background; all excitatory; inhibitory) is shown in figure 10. Before stimulation all neurons in the network are spontaneously active; however, this activity is primed by the learning process: neurons in the foreground of any of the learned stimuli have a higher activity (about 15 s$^{-1}$) compared to the average spontaneous activity in the excitatory network (about 10 s$^{-1}$). This is seen in figure 10, comparing the prestimulus activity in the top window with that in the successive ones. Yet this activity is not selective, i.e. the average rate of neurons selective to any of the learned stimuli is essentially the same.

| Table 2. Parameters used in simulating the structured network (figures 9 and 10). |
|---------------------------------|--------|--------|--------|--------|--------|
| Neuronal parameters            | $E$    | $I$    |        |        |        |
| Number of neurons              | 12 000 | 3000   |        |        |        |
| Synaptic parameters            | $E \rightarrow E$ | $E \rightarrow E$ | $E \rightarrow I$ | $E \rightarrow I$ | $E \rightarrow I$ |
| $J_0 = J_{EE} - \delta J_0$    |        |        |        |        |        |
| $J_1 = J_{EE} + \delta J_1$    |        |        |        |        |        |
| Average efficacy (mV)          | 0.10   | 0.26   | 0.36   | 0.21   | 0.63   |

Figure 9. (a) Spike rasters of 20 excitatory neurons. From top to bottom: five foreground and 15 background neurons. (b) Rasters of 10 inhibitory neurons. The trial protocol is indicated below: P, prestimulus; S, stimulus; D, delay.
Figure 10. Temporal evolution of global activity (in Hz as in figure 3) in different neuronal populations in a network stimulated by a familiar stimulus. Windows: foreground of presented stimulus (neurons with 'visual' response); background; all excitatory neurons (E); inhibitory neurons (I). Each window represents the population averaged activity per 0.5 ms, together with temporal averages in each of the three intervals of the trial: prestimulus, 0–100 ms; stimulus, 100–200 ms; poststimulus, 200–500 ms. Before stimulation neurons in the foreground of any stimulus have a higher spontaneous activity. Note the fast activation of foreground neurons during the stimulus presentation. After removal of the stimulus, the network stabilizes in a 'memory state' in which foreground neurons are active at higher rates. Note that these states are stable in spite of the large fluctuations in the global activity, as in the spontaneous state.

Upon stimulation† by one of the learned stimuli (testing), the stimulated neurons become quickly (in about 5 ms) highly active (about 140 s$^{-1}$). Such fast activation is due to the fact that spontaneous activity 'prepares' the foreground neurons to activation, by placing them

† Since the learning transition probabilities are low, testing can be assumed to take place at constant synaptic matrix.
closer to threshold. Finite synaptic time constants can slow down the neuronal activation (Treves 1993). The other excitatory neurons see their activity lowered from 9 s\(^{-1}\) to about 7 s\(^{-1}\), while inhibition increases from 19 s\(^{-1}\) to 32 s\(^{-1}\).

After the stimulus is removed the network reaches, again very rapidly, a 'working memory state' correlated with the stimulus, as can be seen in figure 10. The foreground neurons stay active in this state at levels of about 80 s\(^{-1}\), while the other excitatory neurons stay at about 7 s\(^{-1}\). The inhibitory activity is about 25 s\(^{-1}\). This state is stable for several seconds, despite the fact that the large fluctuations of the global activity of the unstructured network persist in the memory states.

As emphasized in the introduction, all rates (spontaneous, during stimulation, in delay period) are relatively high. This is because the networks are relatively small. In a network of 100 000 neurons we expect the rates to be lower.

### 3.5. Tests related to network size

Connectivities (hence transmission probabilities) and spike rates were increased to reproduce afferent spike statistics of biological situations in networks practicable for detailed simulations. To test the effects of these variables rescaling on various observable quantities while maintaining the afferent statistics, requires increasing the size of the networks. One is severely constrained in the size of networks with fixed synaptic structure that can be simulated. On the other hand, much larger variable random ('annealed') networks can be simulated, reaching the size of a cortical column. Wherever possible we have done both. Then we passed to larger sizes with variable random networks. Arguments and experiments justifying this procedure are given in appendix D.

#### 3.5.1. CCs versus transmission probability

We performed simulations at different values of \(\epsilon\), keeping the average number of spikes arriving at a neuron and all synaptic parameters fixed. As \(\epsilon\) decreases, \(N\) must be increased to keep \(\epsilon N\) constant. Simulations were run with \(\epsilon \in [0.025, 0.25]\). Correspondingly, the number of neurons \(N \in [4.8 \times 10^4, 4.8 \times 10^5]\), see figure 11. If the spike emission processes of all neurons in the network were uncorrelated, the dynamics would not depend on \(\epsilon\) but only on \(\epsilon N\), the effective number of connections received by a neuron. The simulations show that this is not quite the case.

For each set of parameters we performed a 10 s simulation, and calculated the average CCs. The main difference between these CCs is the amplitude of the peak at zero delay, \(C_{\alpha\beta}(0)\), relative to the background, i.e. \(C_{\alpha\beta}(t)\) at large \(t\). In figure 11 we plot

\[
R_E = \frac{C_{EE}(\tau = 0)}{C_{EE}(\tau = \infty)}
\]

versus \(\epsilon\). This is a measure of the degree of interdependence of the trains of spikes of different neurons in the excitatory network for a given set of synaptic parameters. The corresponding figures for EI or II CCs show essentially the same behaviour. Figure 11 indicates that \(R_E\) decreases linearly to 1 as \(\epsilon \to 0\).

The average frequencies vary mildly (by less than 10%) with \(\epsilon\), for \(\epsilon\) in the range 0–0.3. This is rather surprising, since as \(\epsilon \to 0\), the neurons become uncorrelated, while for finite \(\epsilon\) correlations are present. In fact, the sharp fluctuations in the global activity, which produce the peak in the cross-correlations, are strongly affected by the variation of \(\epsilon\). The surges of activity are followed by relatively quiet intervals, caused by the intervening inhibition, and the net effect on rates turns out to be relatively small. The fact that a rather large peak in the CCs has only small effects on the rates is one of the reasons for the good agreement between simulations and theory.
Simulations with other sets of synaptic values confirm that this phenomenon does not depend on the particular set of parameters: $J_{EE}$ was varied from 0.1 mV to 0.4 mV. The behaviour of the CCs as a function of $\epsilon$ remains very similar.

### 3.5.2. Effect of average firing rates.

To check the effect of spike rate scaling on the amplitude on the CCs, simulations were performed varying the average firing rates (in contrast to the low rate neurons selected in subsection 3.3.1), keeping the transmission probability and the average numbers of afferent excitatory and inhibitory spikes arriving at a neuron fixed. Again this is done increasing the number of neurons $N$, while keeping $\nu N$ and $\epsilon$ fixed. The parameters of the simulations and the results are shown in table 3. It shows that the average peak in the CCs increases with decreasing average spike rate, much as for different groups of neurons in a given network. Yet theory predicts quite accurately the firing rates in a network in which the peak in the CCs exceeds two times the background. Thus correlations even at this level have a small influence on firing rates.

<table>
<thead>
<tr>
<th>$N_E$</th>
<th>$N_I$</th>
<th>$\nu_E$</th>
<th>$\nu_I$</th>
<th>$J_{EE}$</th>
<th>$J_{IE}$</th>
<th>$R_E$</th>
</tr>
</thead>
<tbody>
<tr>
<td>6000</td>
<td>1500</td>
<td>10.4</td>
<td>20.8</td>
<td>0.21</td>
<td>0.35</td>
<td>1.83</td>
</tr>
<tr>
<td>12000</td>
<td>3000</td>
<td>5.2</td>
<td>10.4</td>
<td>0.19</td>
<td>0.32</td>
<td>2.39</td>
</tr>
</tbody>
</table>

### 3.5.3. Agreement with theory at different $N$.

Figure 2 demonstrates remarkable agreement of theory (AB97) with experiment (simulation). This agreement is maintained upon varying $N$ from 6250 to 100 000, keeping $\nu/\epsilon$ fixed, as shown in figure 12 (parameters are given in table 1).
the corresponding table) although the correlation coefficient $R_E$ increases from 1.3 to 1.68, in this range.

4. Discussion

4.1. Simulation as experiment and theory

Networks of IF neurons in realistic conditions exhibit a very rich phenomenology, which shows a remarkable similarity with available neurophysiological data at the level of both mean firing rates and spike statistics beyond average rates. Thus, it does not seem necessary to model the individual neuron in great detail to account for currently observed features of cortical spike dynamics \textit{in vivo}.

However, the ‘observables’ related to spike statistics have been observed experimentally mainly in stimulus-driven activity. One of the purposes of this paper was precisely a systematic study of these observables in the unstructured, spontaneous activity, and we find that much of the structure that is observed in stimulus-driven activity is already present in our network in the spontaneous activity state. This calls for a more detailed experimental study of single or multiple spike statistics in spontaneous activity.

It is very rewarding that a simple theory (AB97) captures major aspects of the system quite accurately: it identifies with precision the regions of dynamic stability of the networks; with no fitting parameters it predicts the spike rate distribution; it accurately predicts the level of synaptic potentiation required for selective activity to coexist with spontaneous activity. The simulations confirm the importance of strong inhibitory feedback to control the fluctuations of activity and of the external background currents which ‘thermalize’ the local module. Lowering the relative inhibitory strength eventually renders the network ‘epileptic’: all neurons spike at very high rates. Above a critical value of inhibition, low spontaneous activity is stable. The effect is very robust, and \textit{no fine tuning of inhibition versus excitation is required} (AB97). The same robustness is found with respect to the variation of external currents: the spontaneous state is stable to such variations, though average rates vary with the external currents. When these currents alone provoke a depolarization which is significantly lower than the threshold, the network may transit into an almost silent state. All these effects are predicted quantitatively by theory.
We have found that in networks with a low ‘transmission probability’, correlations between spike emission processes, as expressed by cross-correlations, influence rates weakly. Another indication that these correlations, of experimental magnitudes, are effectively small is the excellent agreement of the rate distribution with theory. We find that CCs are essentially independent of the synaptic connectivity of the particular pair of neurons. This finding is quite important for experiments that try to deduce information about the synaptic structure from CCs. CCs depend more strongly on firing rates: neurons with low firing rates have more correlated spike emission processes than neurons with high rates. Delays appear to have a strong influence on the time constants of the damped oscillations in the CCs. We have also found that the dynamics of the network is largely independent of the implementation of synaptic disorder, at equal ‘transmission probability’. Networks with fluctuating, unreliable synapses have similar dynamics as networks with fixed, dilute synapses. This could be very useful for the simulation of realistically large cortical modules on modest computers.

4.2. Comparison with neurophysiological data

4.2.1. Distribution of firing rates in spontaneous activity. A rather wide distribution of firing rates in spontaneous activity is usually observed in extracellular recordings in cortex (see, e.g., Koch and Fuster 1989). In both theory and simulations a wide distribution of rates stems from the variability in the connectivity from neuron to neuron. Other parameters such as the variability of intrinsic neuronal parameters like the integration time constant would increase this variability.

4.2.2. Rates in ‘memory states’ versus rates in spontaneous activity. We have presented a single example of selective activity following learning. More detailed account of these states of the network will be given separately. Rates were chosen to be high, to counterbalance the average number of synapses per neuron, which is lower than in a cortical module. Also the coding level $f$ in a memory could not be lowered too much, since a critical number of neurons of the order of several hundreds is necessary to sustain a memory state. Already at this preliminary stage the ratio between firing rates in selective and spontaneous activity is rather low, of order 5. This ratio is not very far from what is observed in delay match to sample experiments (see, e.g., Nakamura and Kubota 1995, Williams and Goldman-Rakic 1995). To check that memory states with rates and coding levels similar to what is observed in experiments in IT or prefrontal cortex are stable, much larger networks would be required. The end product, of course, should be a validation that a simple theory can accurately account for the phenomenology in a wide range of parameters, eliminating the need for future simulation.

4.2.3. Single-cell spike statistics. Recent papers on the variability of cortical neurons have focused on stimulus-driven activity (see, e.g., Softky and Koch 1993). The present study predicts that also when spontaneously active, neurons exhibit a high variability of ISIs, since firing occurs upon unusually high fluctuations of the membrane potential and is similar to a Poisson process. The precise value of the coefficient of variability depends on the relative value of the average depolarization and the post-spike potential.

4.2.4. Cross-correlations. CCs of nearby neurons measured in vivo often exhibit a central peak at zero delay (Kruger and Aiple 1988, Ts’o et al 1986, Gochin et al 1991 Abeles et al
The use of different types of normalizations makes it difficult to make quantitative comparisons for the size of the central peak. Where they can be performed, peaks are of the same order of magnitude as in our simulations. An important problem is the fact that in order to estimate reliably CCs of a single pair of low-firing neurons, a very long recording is necessary. Peak sizes 50% above background would not be detected in data like that of Abeles et al (1995), which is hundreds of seconds long. Again, though most CCs are recorded in stimulus-driven activity, we predict the central peak should already be present in spontaneous activity states.

Our network exhibits high-frequency oscillations in the global activity ranging from about 25 Hz to 200 Hz depending on synaptic delay and conductance time constant parameters. The lower-frequency range is reminiscent of the so-called gamma oscillations in neocortex and hippocampus, whereas the high-frequency range is characteristic of the ‘sharp waves’ observed in hippocampus (Buzsaki 1986, Buzsaki et al 1992, Ylinen et al 1995). CCs with damped oscillations, similar to those found in our simulations, have been observed in visual cortex (e.g. Kreiter and Singer 1996), though rates in the experiment are higher, and the CCs are stimulus-dependent. The discussion of these similarities and differences is beyond the present account (see also Amit 1997). Note that the fast temporal structure might be experimentally difficult to identify, given the length of typical recordings. Central peaks of experimental CCs often have widths of 10–50 ms, larger than the CCs shown in figure 5. However, the width is sensitive to neuronal and synaptic time constants, as shown in figure 8, as well as to structured activity, a subject for future study.

The rate dependence of CCs appears in agreement with Abeles (et al 1995). They find that the most significant peak is obtained for the lowest firing rates of both neurons. It seems also that the sizes of the peaks rank according to firing rates, as in the simulations. This is a prediction which has not yet been systematically explored experimentally. The same rate dependence results also from the more complex network simulated by Hansel and Sompolinsky (1996).

4.3. Comparison with other models of spiking neurons

We conclude with comments comparing the present model with several models of spiking neurons proposed recently:

4.3.1. Single-cell spike statistics. Usher et al (1994) have studied a network of IF neurons with a centre surround synaptic structure, as a candidate solution to the high variability observed in single-cell distributions of interspike intervals (ISI), in a network with high rates, as in primary visual cortex. Tsodyks et al (1994) proposed other solutions to the variability problem, studying in detail a single neuron receiving a random input. One is related to the possibility that post-spike reset polarization is above the average depolarization level (see also Troyer and Miller 1997). Here we have confirmed that this hypothesis is valid in a network of spontaneously active, interacting elements. However, our ISI histograms are quite stereotyped and all look exponential-like, in contrast to those of Hansel and Sompolinsky (1996). The bimodal ISI histograms characteristic of bursting neurons could probably be obtained with random rather than fixed, post-spike reset potential. It may be, though, that this feature does depend on specific ion-channel dynamics which lead to systematic bursts.

4.3.2. Synchronization. The cross-correlations reported here are rather similar to the ones observed in Usher et al (1994), Tsodyks and Sejnowski (1995) and Hansel and Sompolinsky.
Dynamics of a recurrent network of spiking neurons

(1996). The difference between our paper and the studies of Usher et al (1994) and Tsodyks and Sejnowski (1995) is that we have investigated extensively the behaviour of CCs as a function of many network parameters. Our paper also differs from that of Hansel and Sompolinsky (1996) in the interpretation of CCs. An important question raised by Ginzburg and Sompolinsky (1994) and Hansel and Sompolinsky (1996) is the criterion for synchrony in a given network state. They suggest that if the central peak in the CCs disappears into the background in the limit of infinitely many neurons, the network is asynchronous. If the peak stays above the background, it is defined as synchronous. In our networks there is no such clear-cut distinction: it would be considered asynchronous if the number of connections per neuron was kept fixed in the limit \( N \to \infty \); it would be mildly synchronous if the 'transmission probability' were held fixed. Our conclusion is that any network with excitatory and inhibitory neurons with recurrent connections is likely to have a finite degree of correlation in spike emission processes, expressed in the central peak of the CCs. However, for realistic levels of transmission probability, these correlations are effectively small, as witnessed by the fact that these correlations only weakly influence rates.

Finally, we point out some important differences with the above-mentioned models: our network has no geometrical structure; the dynamics of the neural assembly is studied in the absence of the driving stimulus, though the activity in the network might have been provoked by a stimulus; structured delay activity is studied in conjunction with the stability of the underlying spontaneous activity; it models no predetermined function, but follows the autonomous spike dynamics sustained by the synaptic structure and their development as a consequence of a specific learning dynamics; the synaptic structure is either unformed or structured by well-defined synaptic dynamics generated by external stimuli; it aims at both qualitative and quantitative phenomena observed in such regions as inferior-temporal cortex; and, most important, it shows that the outcome of such dynamics can be predicted by an analytical theory.

Acknowledgments

We are indebted to Stefano Fusi for very helpful discussions in the early stages of this work, and to Misha Tsodyks and Yali Amit for comments on the manuscript. DJA’s research has been supported in part by a Human Capital and Mobility grant of the EEC. NB acknowledges a fellowship of Programme Cognisciences, CNRS, France, and the hospitality of INFN, Università di Roma, where this work was started.

Appendix A. Stable rates in a homogeneous unstructured network

In a network of IF neurons the self-reproducing spike rates for excitatory and inhibitory populations are given by the solutions of the coupled equations

\[
\nu_E = \phi_E(\mu_E, \sigma_E) \tag{A1}
\]

\[
\nu_I = \phi_I(\mu_I, \sigma_I) \tag{A2}
\]

in which the means \( \mu_\alpha \) and SDs \( \sigma_\alpha \) (\( \alpha = (E, I) \)) of the synaptic inputs are functions of the rates of the excitatory and the inhibitory neurons, \( \nu_E \) and \( \nu_I \), via

\[
\mu_E = \epsilon \tau_E (N_E \nu_E J_{EE} - N_I \nu_I J_{EI}) + I_{ext}^E \tag{A3}
\]

\[
\sigma_E^2 = \epsilon \tau_E (N_E \nu_E J_{EE}^2 + N_I \nu_I J_{EI}^2) + J_{EE} I_{ext}^E \tag{A4}
\]
\[ \mu_I = \epsilon \tau_I (N_E v_E J_{IE} - N_I v_I J_{II}) + I^{\text{ext}}_I \]  \hspace{1cm} (A5)

and

\[ \sigma^2_I = \epsilon \tau_I (N_E v_E J^{2}_{IE} + N_I v_I J^{2}_{II}) + J^{2}_E I^{\text{ext}}_I. \]  \hspace{1cm} (A6)

The transduction function \( \phi_\alpha \) of \( \alpha \) neurons (Tuckwell 1988, Amit and Tsodyks 1991) is

\[ \phi_\alpha(\mu_\alpha, \sigma_\alpha) = \left( \tau_{\text{ARP}} + \tau_\alpha \int_{(0-\mu_\alpha)/\sigma_\alpha}^{(\theta-\mu_\alpha)/\sigma_\alpha} \psi(u) \, du \right)^{-1} \]  \hspace{1cm} (A7)

with \( \psi \) given by

\[ \psi(u) = \sqrt{\pi} \exp(u^2) \left[ 1 + \text{erf}(u) \right] \]  \hspace{1cm} (A8)

and \( \tau_{\text{ARP}} \) is the absolute refractory period.

**Appendix B. Stable rates in inhomogeneous unstructured networks**

When the number of connections received by a neuron varies from neuron to neuron, as is the case when synapses are chosen randomly and independently between each pair of neurons, the (temporally) averaged rates also fluctuate from neuron to neuron. Mean-field theory (AB97) can be extended to cover this situation and produce the full distribution of rates in the population. Here we give a skeleton description of the theory for completeness. Details will be given elsewhere.

The basic idea is that the spike rate of a cell is determined by the mean depolarization and the variance of the *temporal* course of its depolarization, or in a stationary situation, of the *temporal* course of the mean and variance of its afferent current. These are single-cell variables. Given the cell to cell variability of the connectivity and of the rates, one can estimate the mean and variance of the *population* distribution of afferents over the cells, and hence of the resulting *population* distribution of rates. In a stable situation the resulting distribution should reproduce the assumed one. It must then be checked for stability.

Suppose that the *population* distributions of *temporal* means of the afferents are Gaussian with *population* means for excitatory (inhibitory), \( E \) (\( I \)), neurons \( \mu_{E,I} \) and *population* variances \( \Delta \mu_{E,I}^2 \). In that case the *population* distributions of the mean depolarizations can be written as

\[ \mu_{E,I}(z) = \mu_{E,I} + z \sqrt{\Delta \mu_{E,I}^2} \]  \hspace{1cm} (B1)

with \( z \) a random Gaussian variable of mean zero and unit variance. For simplicity we neglect the variability in the variances of the afferents. Their effect is relatively weak. Such a distribution of means leads to a *population* distribution of rates via:

\[ v_E(z) = \phi_E(\mu_{E}(z), \sigma_E) \quad v_I(z) = \phi_I(\mu_{I}(z), \sigma_I). \]  \hspace{1cm} (B2)

These induced rate distributions have population means and variances given by the Gaussian averages

\[ v_E = \int Dz \ v_E(z) \quad v_I = \int Dz \ v_I(z) \]  \hspace{1cm} (B3)

and

\[ \Delta v_E^2 = \int Dz \ v_E^2(z) - v_E^2 \quad \Delta v_I^2 = \int Dz \ v_I^2(z) - v_I^2. \]  \hspace{1cm} (B4)

where \( Dz = \exp(-z^2/2)dz/\sqrt{2\pi} \). The *temporal* means \( \mu_\alpha(z) \) which enter the computation of the rates, equations (B2), are functions of the *population* averages and of the variances.
of the rates of the excitatory and the inhibitory neurons, via the population averages of the depolarization and of their variances, $\mu_{E,I}, \Delta \mu_{E,I}^2, \sigma_{E,I}^2$, which enter equations (B1). Those, in turn are given by

$$\Delta \mu_E^2 = \tau_E^2 \epsilon \left[ (1 + \Delta^2 - \epsilon)(N_E \nu_E^2 J_{EE}^2 + N_I \nu_I^2 J_{EI}^2) + N_E \Delta \nu_E^2 J_{EE}^2 + N_I \Delta \nu_I^2 J_{EI}^2 \right]$$

and

$$\Delta \mu_I^2 = \tau_I^2 \epsilon \left[ (1 + \Delta^2 - \epsilon)(N_E \nu_E^2 J_{IE}^2 + N_I \nu_I^2 J_{II}^2) + N_E \Delta \nu_E^2 J_{IE}^2 + N_I \Delta \nu_I^2 J_{II}^2 \right]$$

where $\Delta$ measures the spread of the synaptic efficacies and $\mu_{E,I}$ and $\sigma_{E,I}$ are given in terms of the population averaged rates $\nu_{E,I}$ by equations (A3)-(A6). Self-reproducibility of the activity state of the system is the condition that the mean and variances of the induced rate distribution are equal to those of the inducing distribution.

Given the rates as functions of $\tau$, the distribution of rates in both excitatory and inhibitory networks is computed from

$$P_{E,I}(\nu) = \int D\tau \delta(\nu - \phi_{E,I}(\mu_{E,I}(\tau), \sigma_{E,I}))$$

### Appendix C. Synaptic distributions after learning

When $p$ stimuli $\{\eta_{i\mu}\}$ are presented many times in a random order, the probability that the synaptic efficacy $J_{ij}$ ends in its potentiated state is proportional to $q_+$ (the probability that transition occurs upon activation of both neurons) and to $P_{ij}$ (the number of stimuli in the training sequence which tend to potentiate it). The probability of it ending depressed is proportional to $q_-$ and to the number of stimuli $D_{ij}$ which tend to depress it. In terms of the stimuli variables (subsection 2.1.5), $P_{ij}$ and $D_{ij}$ are given as

$$P_{ij} = \sum_{\mu} \eta_{i\mu} \eta_{j\mu}$$

$$D_{ij} = \sum_{\mu} \left[ \eta_{i\mu} (1 - \eta_{j\mu}) + \eta_{j\mu} (1 - \eta_{i\mu}) \right]$$

Since stimuli are shown many times, if at least one of the two neurons $(i,j)$ is activated during the learning process, i.e. $P_{ij} + D_{ij} > 0$, the synaptic efficacy will have made at least one transition. Thus the probability that the synapse stays unmodified is zero, while it is potentiated with probability

$$\frac{q_+ P_{ij}}{q_+ P_{ij} + q_- D_{ij}}$$

and depressed with probability

$$\frac{q_- D_{ij}}{q_+ P_{ij} + q_- D_{ij}}$$

If $P_{ij} + D_{ij} = 0$ the synaptic efficacy is not modified with probability one. In the simulations we used $q_+ = 0.1, q_- = 0.025$.

### Appendix D. Comparison of different types of synaptic disorder

Simulations of networks with fixed connectivity require storing the full synaptic matrix. Memory sets a limit of about 15 000 neurons on a workstation. A network with variable connectivity requires no memory for the synaptic matrix, which allows the simulation of networks with up to $10^5$ neurons, at which point the time constraint intervenes. Hypotheses related to the size of the network up to biological sizes can be tested on networks with variable connectivity. In order to be able to employ this expedient two issues have to be investigated:
1. Variable networks are inherently uniform, i.e. all neurons are equivalent with respect to the connectivity and transmission of spikes. Their dynamics would naturally be compared to that of networks with fixed connectivity generated by procedure A of subsection 2.1.3 (fixed random connectivity).

2. Realistic networks are at least partially ‘quenched’ and are not uniform. One must compare the dynamics of uniform versus non-uniform networks with fixed connectivity.

We have performed simulations to compare the spike dynamics of homogeneous networks with ‘quenched’ and ‘annealed’ types of disorder. We find that the network dynamics depends mostly on the ‘transmission probability’ $\epsilon$. Two limits were compared: full quenching ($c = \epsilon$, $r = 1$) and full annealing ($c = 1$, $r = \epsilon$). The delays were chosen accordingly. The transmission probability $\epsilon$ varied in the range 0.1–0.3, and the excitatory-to-excitatory average PSP, $J_{EE}$, in the range 0.1–0.4 mV. Annealed and quenched networks of type A produce in all cases very similar results for both firing rates in excitatory and inhibitory populations and for average CCs. In all cases in which it was feasible to perform simulations of a quenched network (i.e. $\epsilon$ not too small), results were essentially identical to the annealed case. This is shown by the proximity of the + and the ♦ in figure 11. Similar results hold for average firing rates.

Simulations were then performed to test the effect of homogeneity on the dynamics of the network. Synaptic matrices were generated according to procedures A and B of subsection 2.1.3. In procedure A all neurons have an equal number of afferent synapses. In procedure B (variable random connectivity) the number of afferent synapses varies from neuron to neuron. The parameters of both networks are given in table 1. The measured excitatory spike rates in the homogeneous network (about 11 s$^{-1}$) are somewhat lower than in the inhomogeneous network (about 13.6 s$^{-1}$). Both are in close agreement with the theoretical prediction (10.4 s$^{-1}$ and 13.1 s$^{-1}$, respectively). The rates in the homogeneous network are, of course, uniform, in contrast with the wide distributions observed in figure 2. These are the main differences observed between the two networks. ISI distributions and CCs are very similar in both cases. The central peak in the cross-correlations is slightly higher in the case of the homogeneous network, which can be attributed to the lower average firing rate. This similarity is observed in all quantities measured.

References


Amit D J 1995 The Hebbian paradigm reintegrated: local reverberations as internal representations Behav. Brain Sci. 18 617


—— 1997 Model of global spontaneous activity and local structured activity during delay periods in the cerebral cortex Cerebral Cortex 7 237


Artola A and Singer W 1993 Long-term depression of excitatory synaptic transmission and its relationship to long-term potentiation Trends Neurosci. 16 480
Bliss T V P and Collingridge G L 1993 A synaptic model of memory: long-term potentiation in the hippocampus Nature 361 31
Braitenberg V and Schütz A 1991 Anatomy of the Cortex (Berlin: Springer)
Brunel N and Sergi S 1997 Firing frequency of integrate-and-fire neurons with finite synaptic time constants, in preparation (see http://www.lps.ens.fr/~brunel)
Buzsaki G 1986 Hippocampal sharp waves: their origin and significance Brain Res. 398 242–52
Fuster J M 1995 Memory in the Cerebral Cortex (Cambridge, MA: MIT Press)
Knight B W 1972 Dynamics of encoding in a population of neurons J. Gen. Physiol. 59 734
Koch K W and Fuster J M 1989 Unit activity in monkey parietal cortex related to haptic perception and temporary memory Exp. Brain Res. 76 292
Komatsu Y, Nakajima S, Toyama K and Fetz E 1988 Intracortical connectivity revealed by spike-triggered averaging in slice preparations of cat visual cortex Brain Res. 442 359
Kreier A K and Singer W 1996 Stimulus dependent synchronization of neuronal responses in the visual cortex of the awake macaque monkey J. Neurosci. 16 2381
Kruger J and Aiple F 1988 Multi electrode investigation of monkey striate cortex: spike train correlations in the infragranular layers J. Neurophysiol. 80 798
Lacaille J 1991 Postsynaptic potentials mediated by excitatory and inhibitory amino acids in interneurons of stratum pyramidale of the CA1 region of rat hippocampal slices in vitro J. Neurophysiol. 66 1441
Mason A, Nicoll A and Stratford K 1991 Synaptic transmission between individual pyramidal neurons of the rat visual cortex in vitro J. Neurosci. 11 72
McCormick D, Connors B, Lighthall J and Prince D 1985 Comparative electrophysiology of pyramidal and sparsely spiny stellate neurons in the neocortex J. Neurophysiol. 54 782
Miyashita Y 1988 Neuronal correlate of visual associative long-term memory in the primate temporal cortex Nature 335 817
Nakamura K and Kubota K 1995 Mnemonic firing of neurons in the monkey temporal pole during a visual recognition memory task J. Neurophysiol. 74 162
Rapp M, Yarom Y and Segev I 1992 The impact of parallel background activity on the cable properties of cerebellar Purkinje cells Neural Comput. 4 518
Softky W R and Koch C 1993 The highly irregular firing of cortical cells is inconsistent with temporal integration of random EPSPs J. Neurosci. 13 334
Thomson A, Deuchars J and West D 1993a Single axon excitatory postsynaptic potentials in neocortical interneurons exhibit pronounced paired pulse facilitation Neuroscience 54 347
Thomson A, West D and Deuchars J 1993b Single axon IPSPs elicited by morphologically identified interneuron in rat neocortex in vitro J. Physiol. (London) 473 173
Treves A 1993 Mean-field analysis of neuronal spike dynamics Network: Comput. Neural Syst. 4 259
Troyer T W and Miller K D 1997 Physiological gain leads to high ISI variability in a simple model of a cortical regular spiking cell Neural Comput. 9 971
Ts’o D Y, Gilbert C D and Wiesel T N 1986 Relationships between horizontal interactions and functional architecture in cat striate cortex as revealed by cross-correlation analysis J. Neurosci. 6 1160
Tuckwell H C 1988 Introduction to Theoretical Neurobiology (Cambridge: Cambridge University Press)
Usher M, Stemmler M, Koch C and Olami Z 1994 Network amplification of local fluctuations causes high spike rate variability, fractal firing patterns and oscillatory local field potentials Neural Comput. 6 795
Williams G V and Goldman-Rakic P S 1995 Modulation of memory fields by dopamine D1 receptors in prefrontal cortex Nature 376 572